

Modelling the evolving ductility of biodegradable polymers

A. Hill¹, K.S. Bezela¹, R.N. Shirazi¹, M. Destrade², W. Ronan¹

¹ Biomechanics Research Centre, Biomedical Engineering, NUI Galway

² School of Mathematics, Statistics and Applied Mathematics, NUI Galway

Postgraduate Modelling Research Group

email: a.hill5@nuigalway.ie

BioMEC

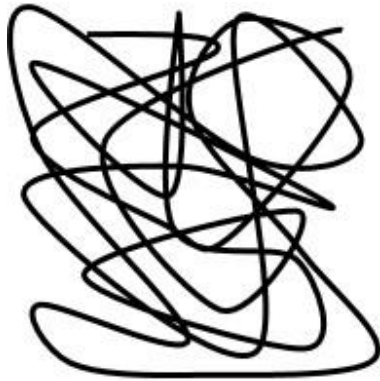
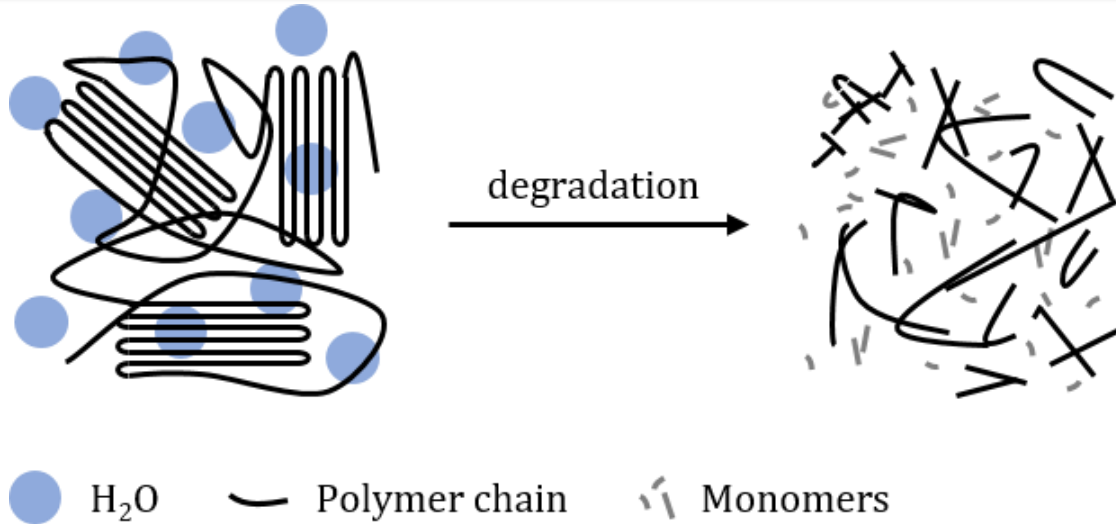


NUI Galway
OÉ Gaillimh

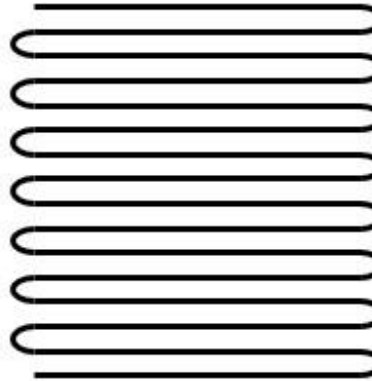
Research objective

- Develop a modelling framework for biodegradable polymers;
- For use in the medical device industry, specifically cardiovascular stents
- Overcome risks associated with metal stents

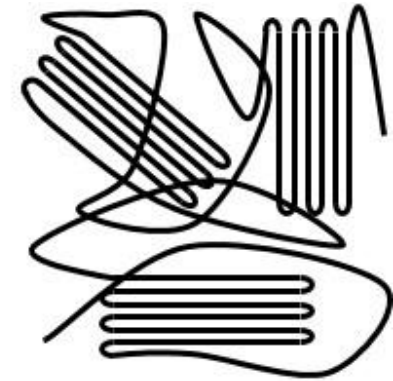
Biodegradable polymers



Amorphous



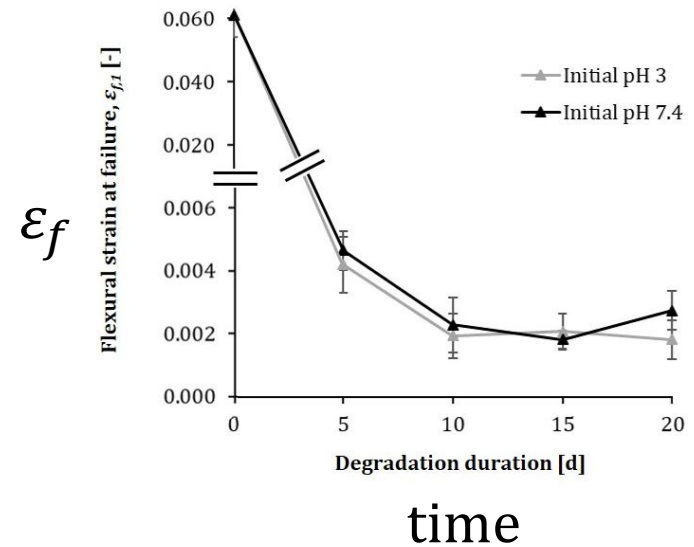
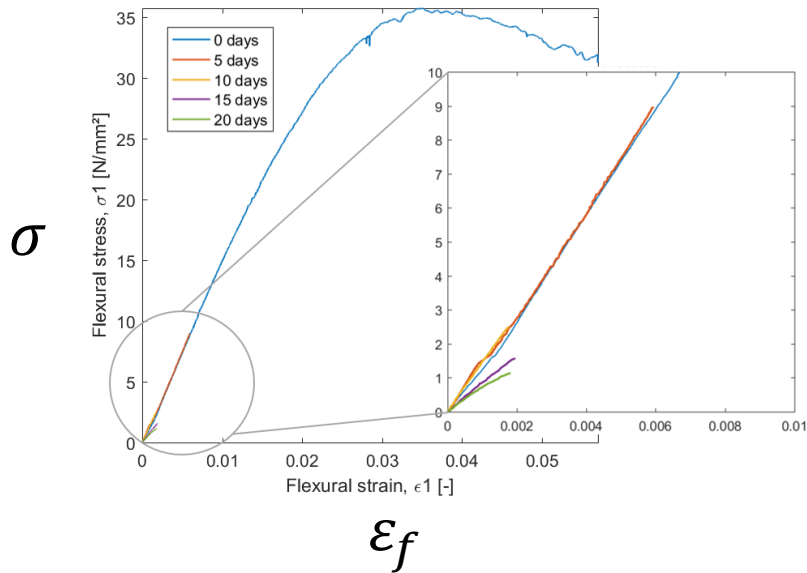
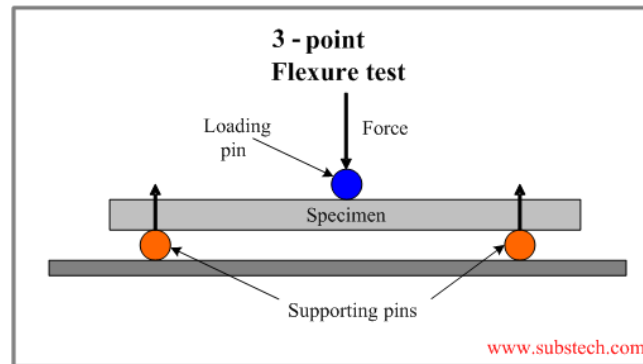
Crystalline



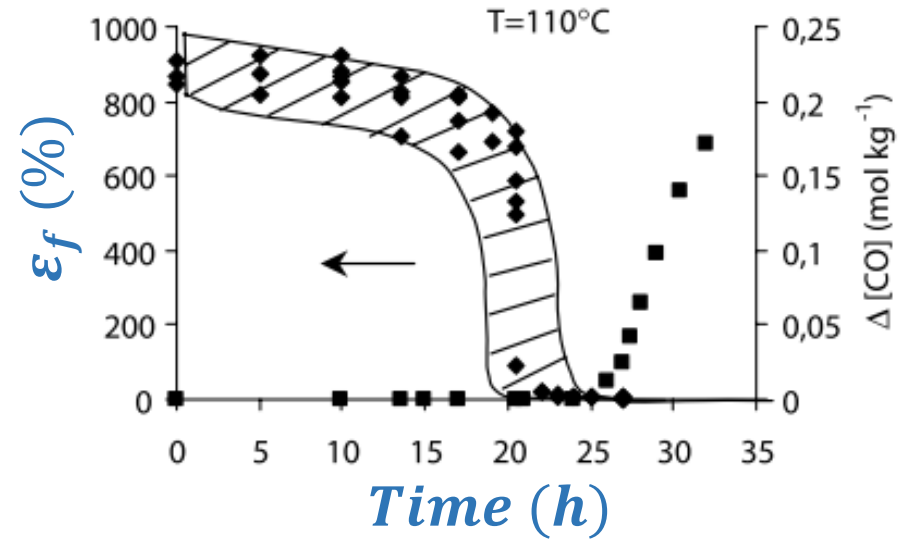
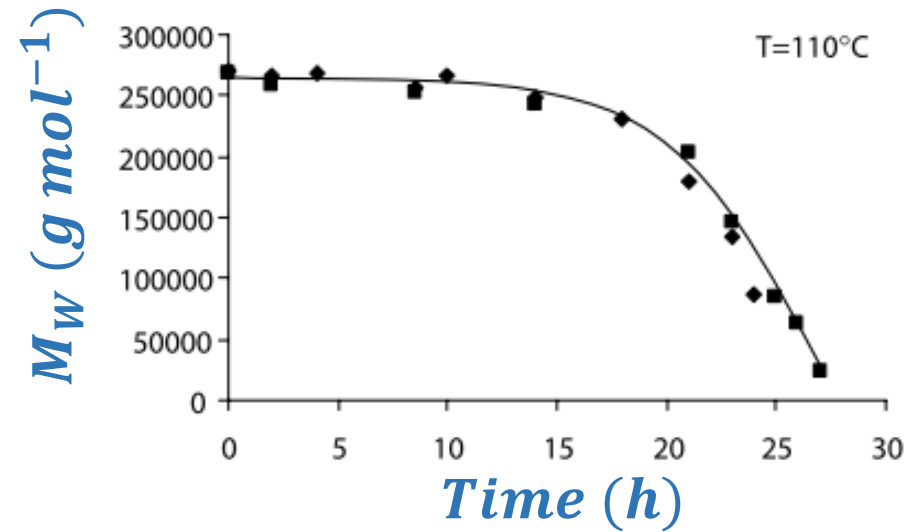
Semi-crystalline

Experimental observations

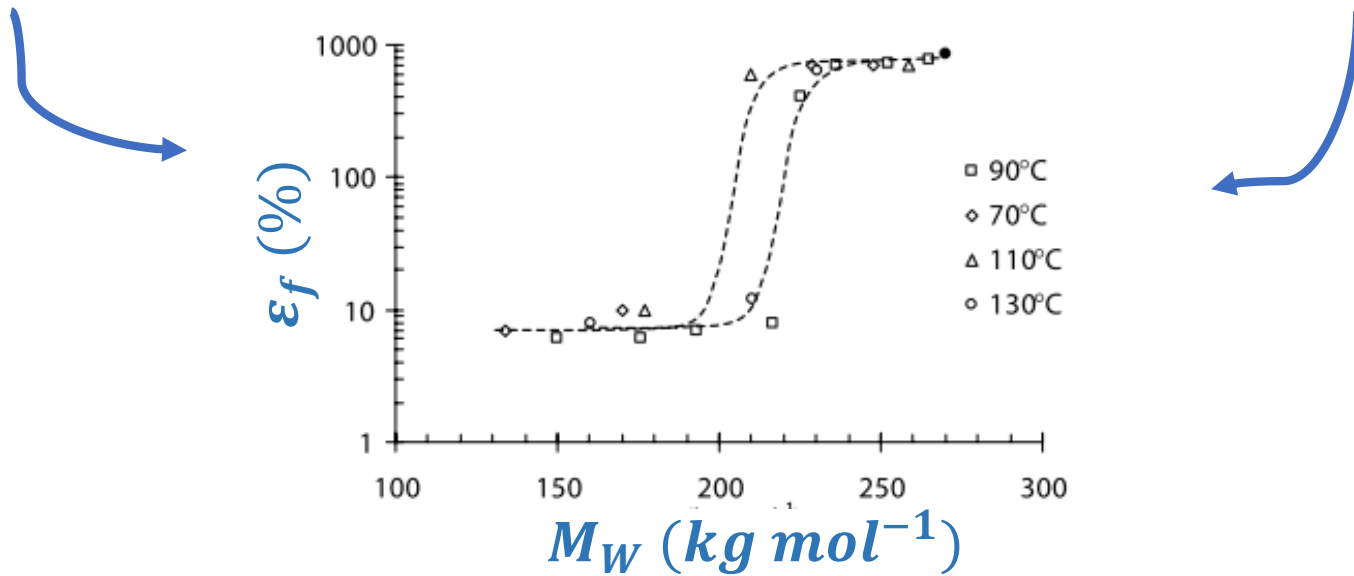
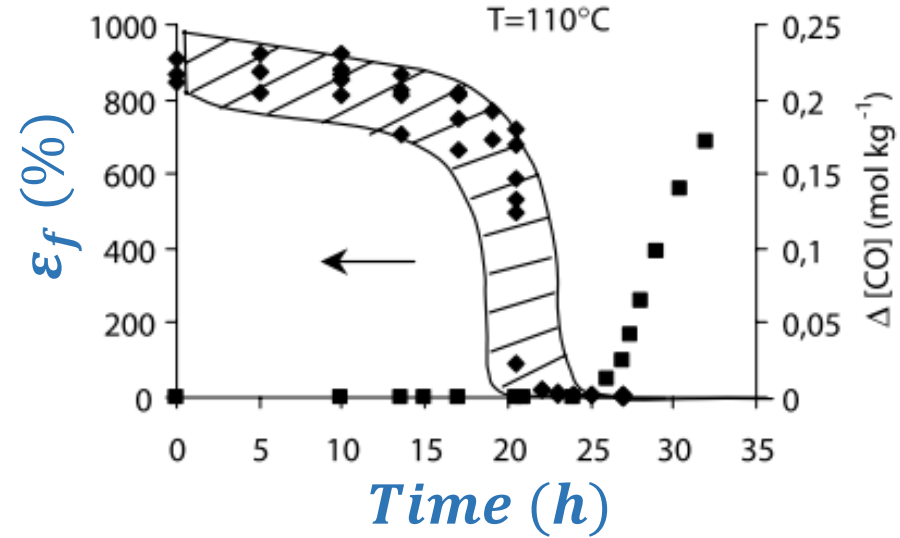
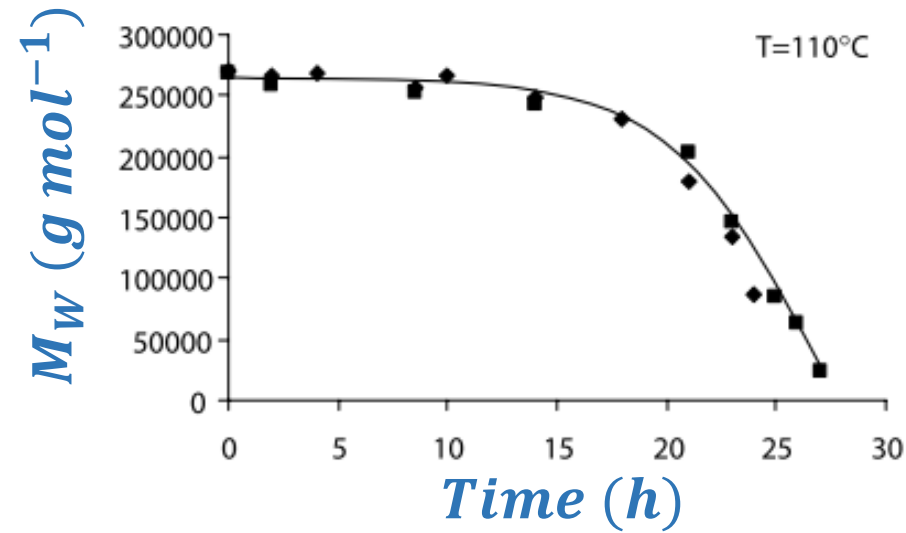
Ductile-to-brittle transition for increasing degradation duration in PLA:



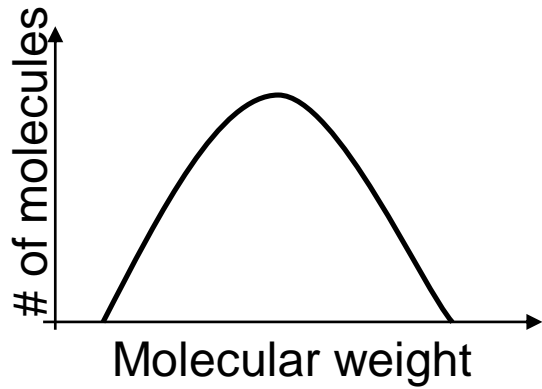
Fayolle et al., 2004



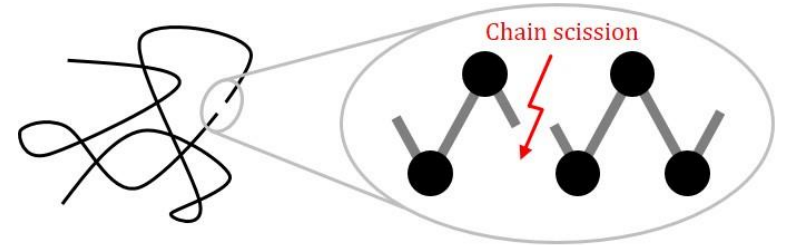
Fayolle et al., 2004



Current work



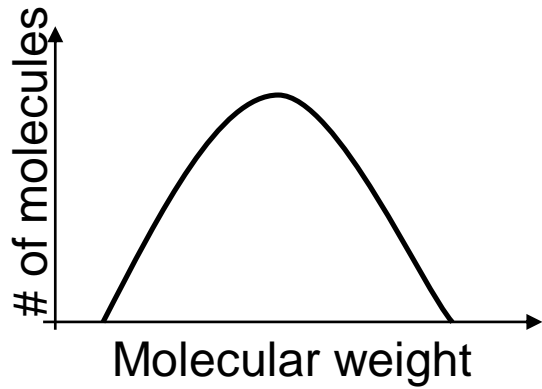
Degradation:



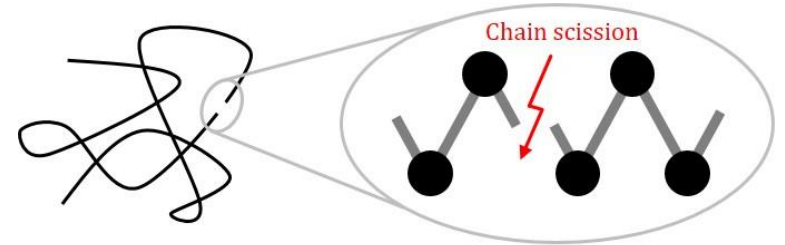
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

Current work



Degradation:



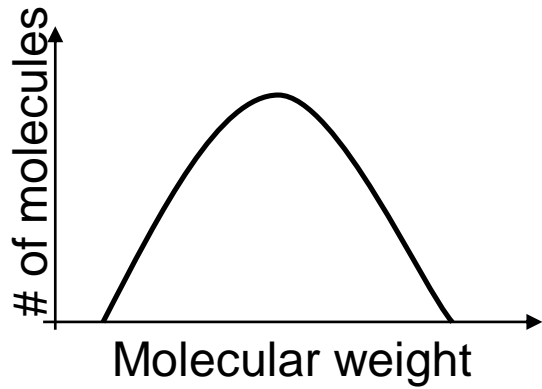
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

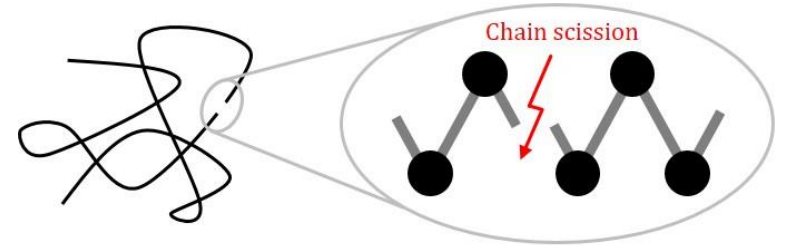
Track chain lengths in MATLAB:

⌈	1000	0	0	...
	1020	0	0	...
	1040	0	0	...
	1060	0	0	...
	1080	0	0	...
	⋮	⋮	⋮	

Current work



Degradation:



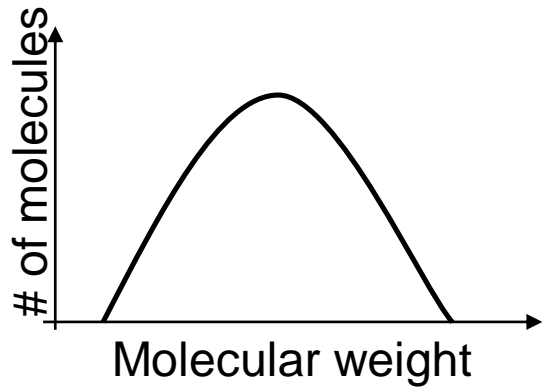
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

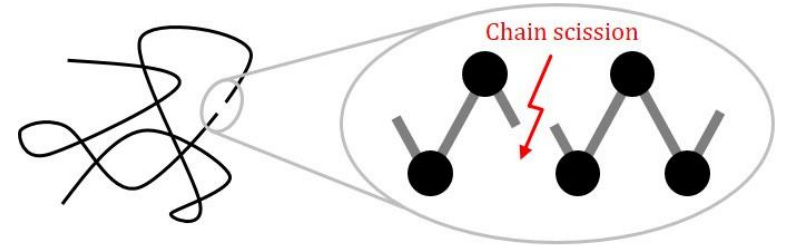
Track chain lengths in MATLAB:

1000	0	0	...
1020	0	0	...
1040	0	0	...
1060	0	0	...
1080	0	0	...
⋮	⋮	⋮	

Current work



Degradation:



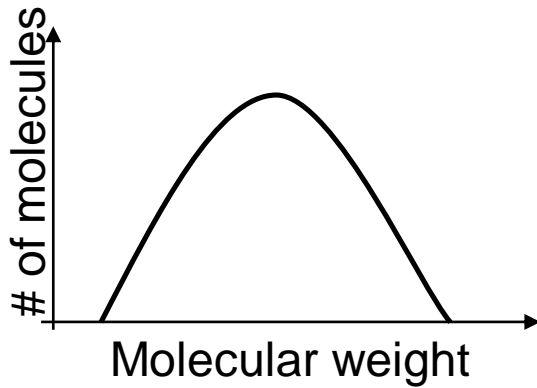
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

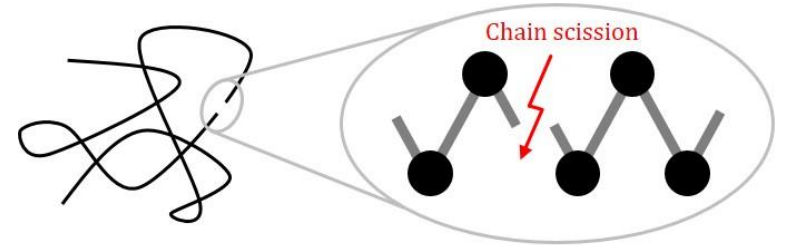
Track chain lengths in MATLAB:

⎛	999	0	0	...
	1020	0	0	...
	400	640	0	...
	1060	0	0	...
	1080	0	0	...
	⋮	⋮	⋮	⋮

Current work



Degradation:



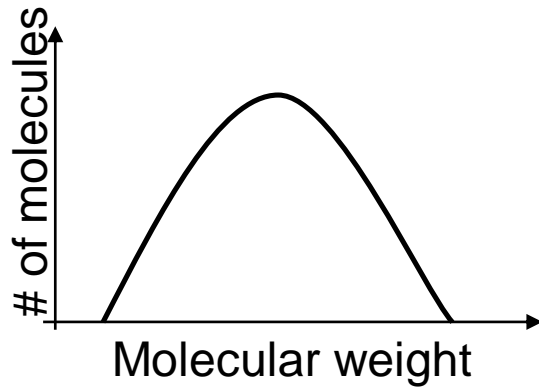
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

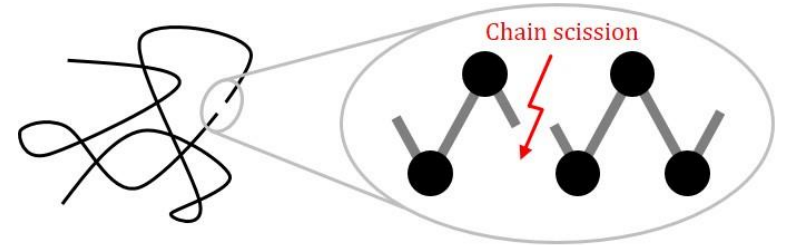
Track chain lengths in MATLAB:

999	0	0	...
1020	0	0	...
400	640	0	...
1060	0	0	...
1080	0	0	...
⋮	⋮	⋮	

Current work



Degradation:



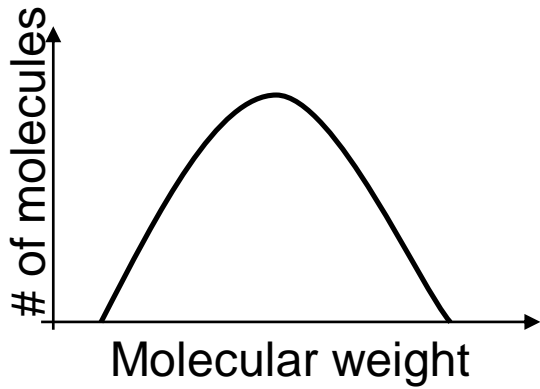
— Polymer chain ● Monomer — Chemical bond

- End scissions
- Random scissions

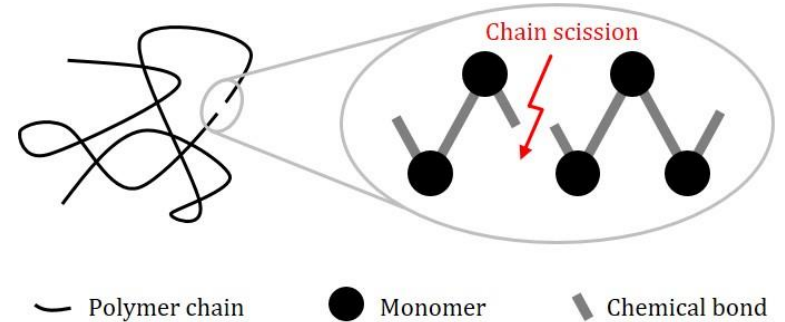
Track chain lengths in MATLAB:

999	0	0	...
1020	0	0	...
398	640	2	...
1060	0	0	...
1079	0	0	...
⋮	⋮	⋮	...

Current work

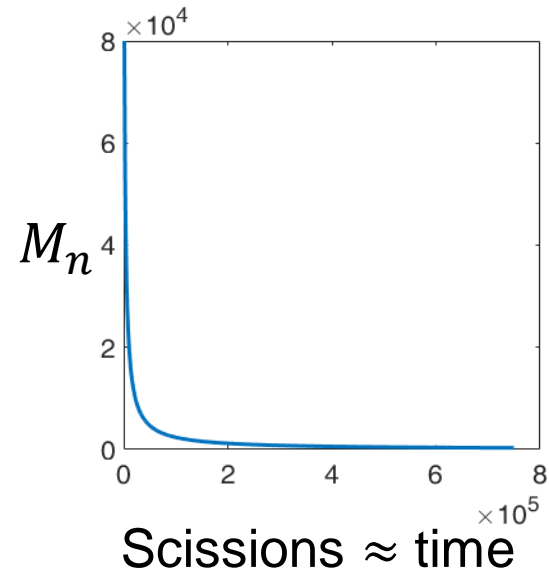


Degradation:

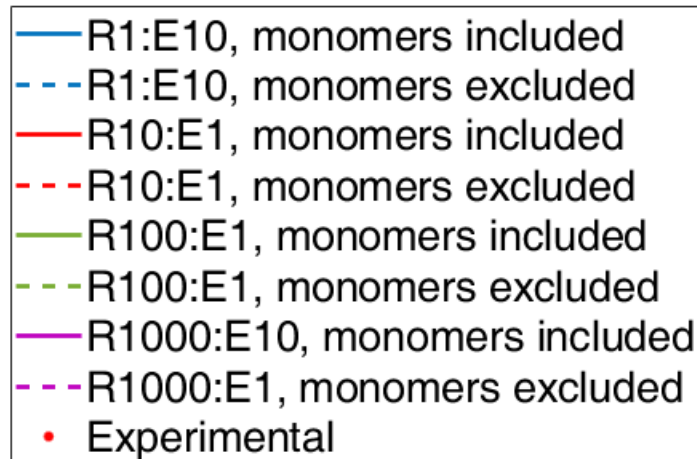
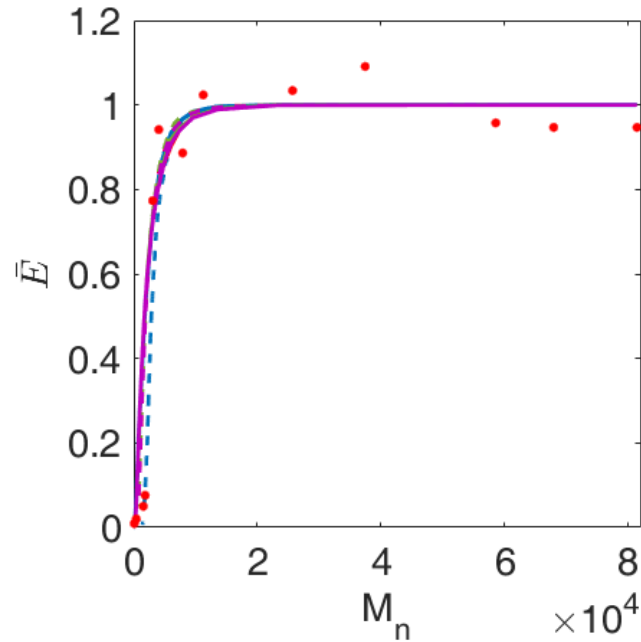
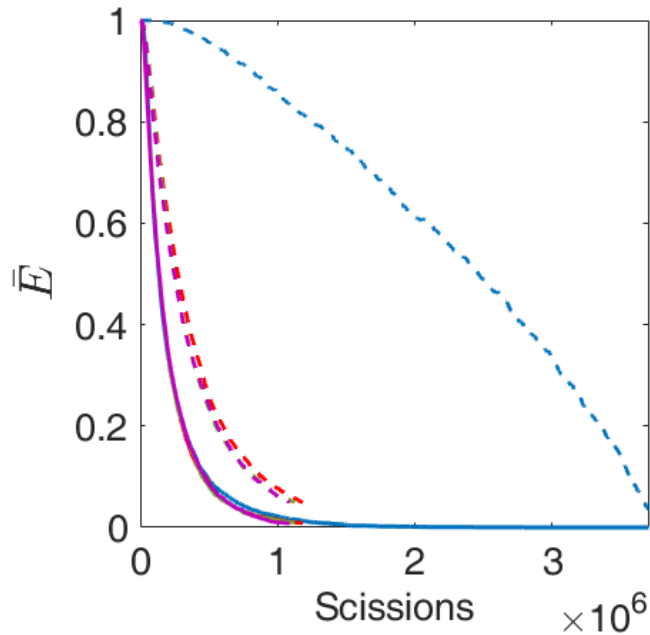


Track chain lengths in MATLAB:

	999	0	0	...
	1020	0	0	...
	398	640	2	...
	1060	0	0	...
	1079	0	0	...
	⋮	⋮	⋮	⋮



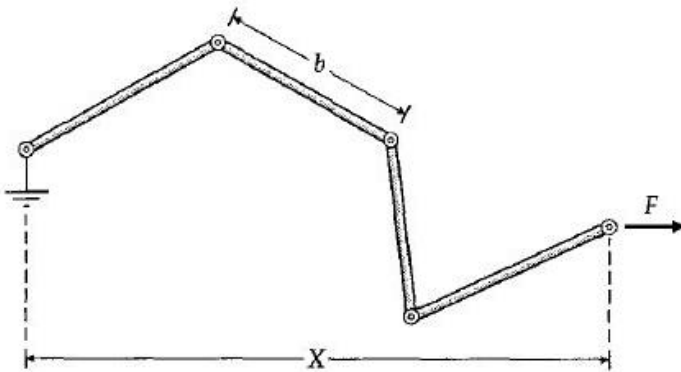
Predicted stiffness



Relating strain failure to polymer units

Freely jointed chain:

- Behaves as entropic spring



$\epsilon_f^{M_n}$ - related to M_n

ϵ_f^N - related to chains above M_n^{crit}

Maximum length of extended chain before failure, $L_f = N$

Root mean-square end-to-end distance, $\sqrt{N} = L_0$

Strain failure, ϵ_f :

Engineering strain:

$$e_f = \frac{L_f - L_0}{L_0} = \frac{N - N^{\frac{1}{2}}}{N^{\frac{1}{2}}} = N^{\frac{1}{2}} - 1$$

True strain:

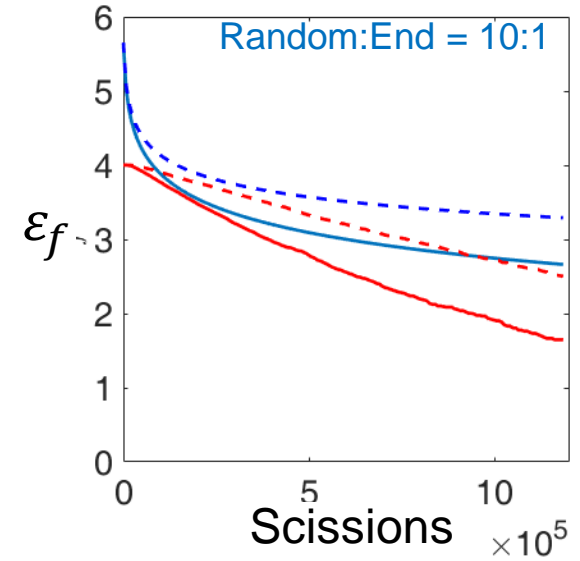
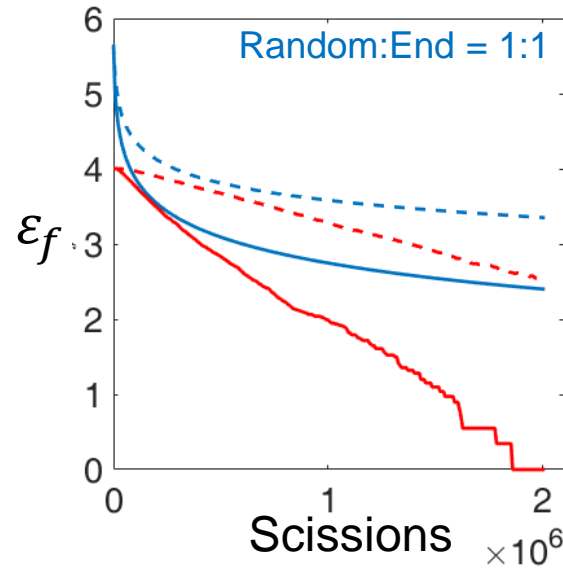
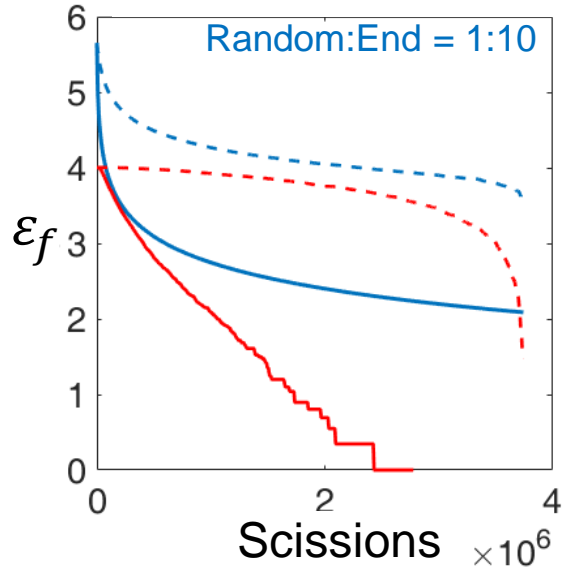
$$\epsilon_f = \ln(1 + e_f) = \frac{1}{2} \ln(N)$$

N = number of polymer units

Results

$\varepsilon_f^{M_n}$
 ε_f^N

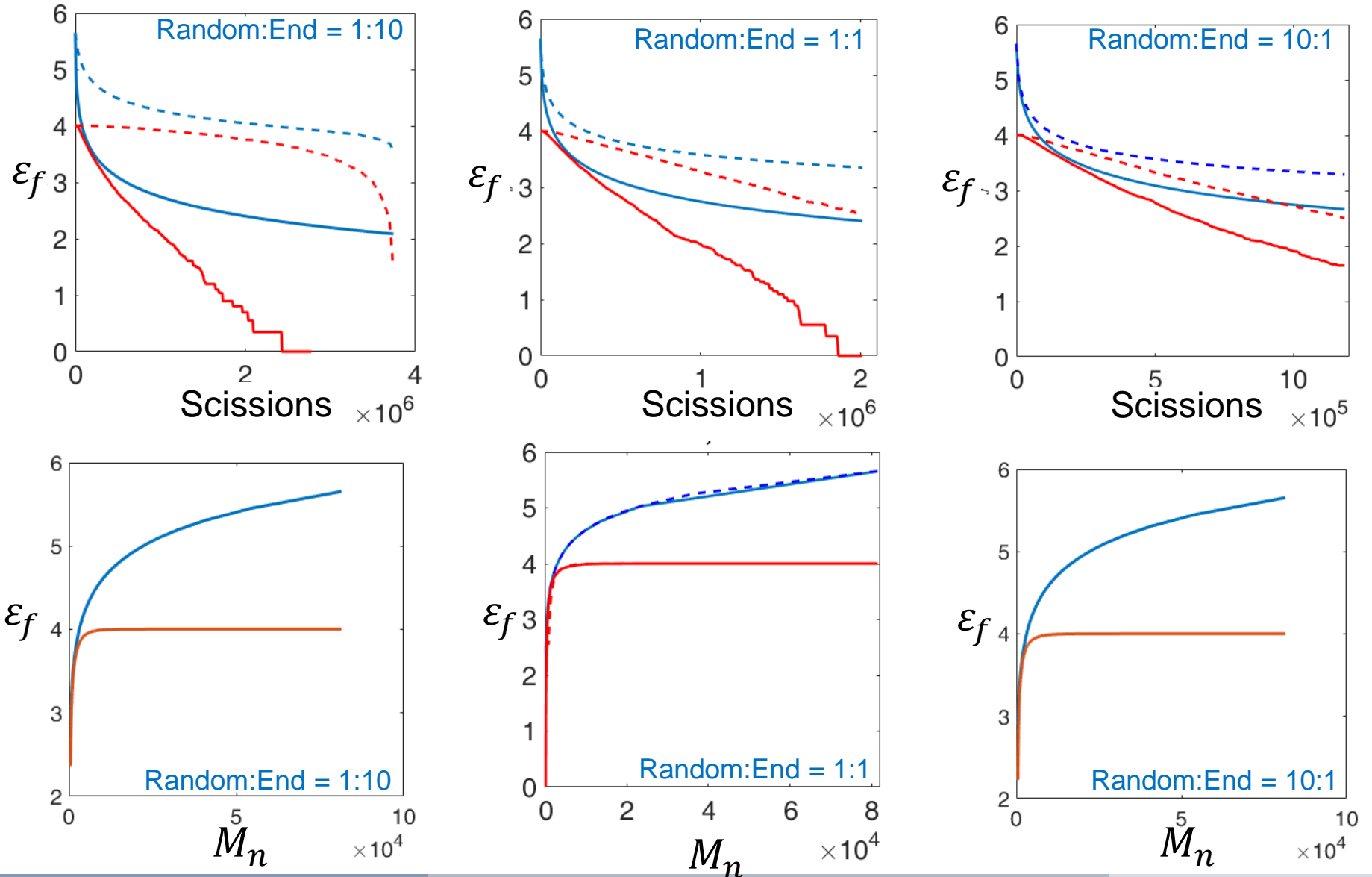
— Monomers included
- - - Monomers excluded



Results

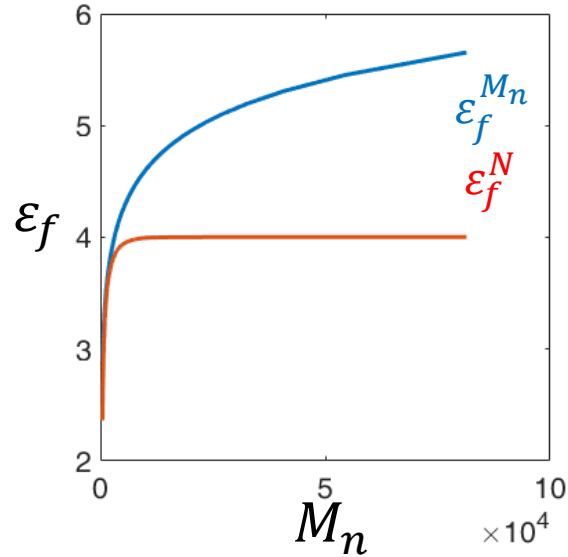
$\varepsilon_f^{M_n}$
 ε_f^N

— Monomers included
 - - - Monomers excluded

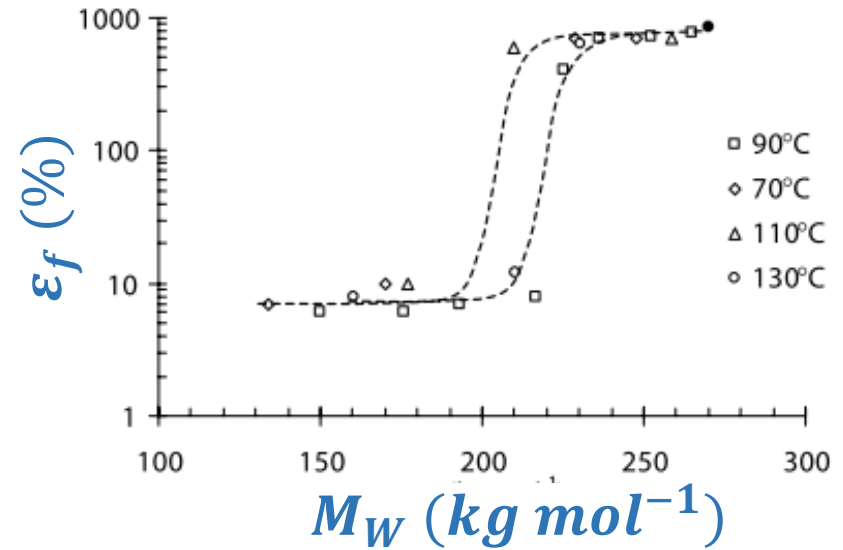


Comparing results

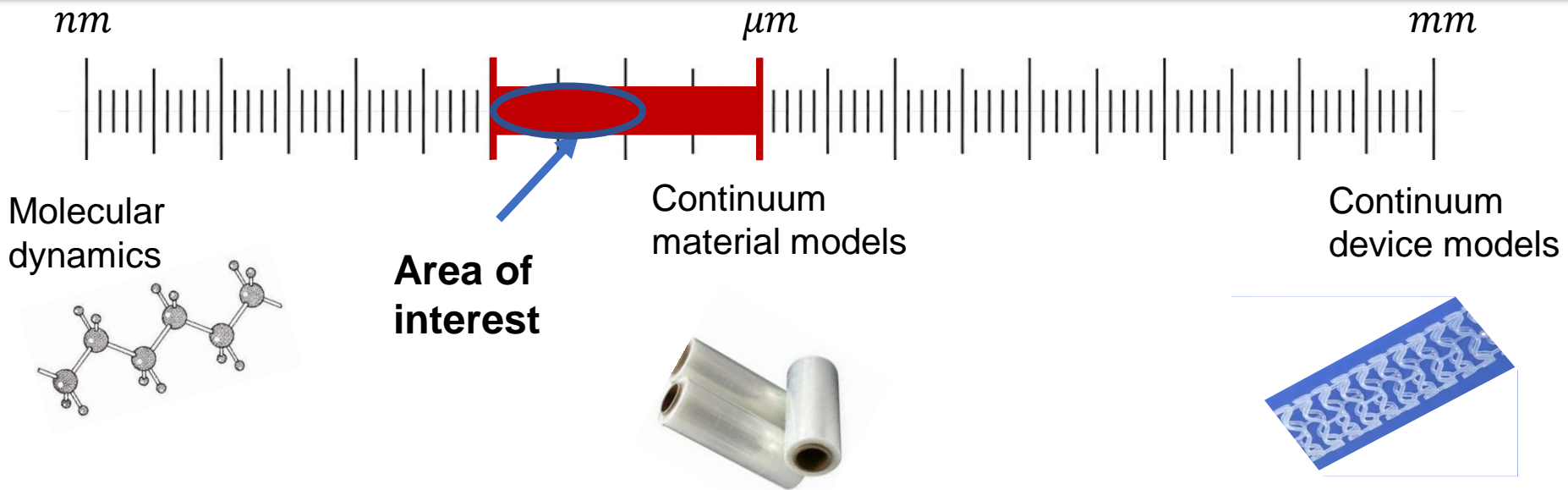
Current results:



Fayolle et al., 2004:



Further work

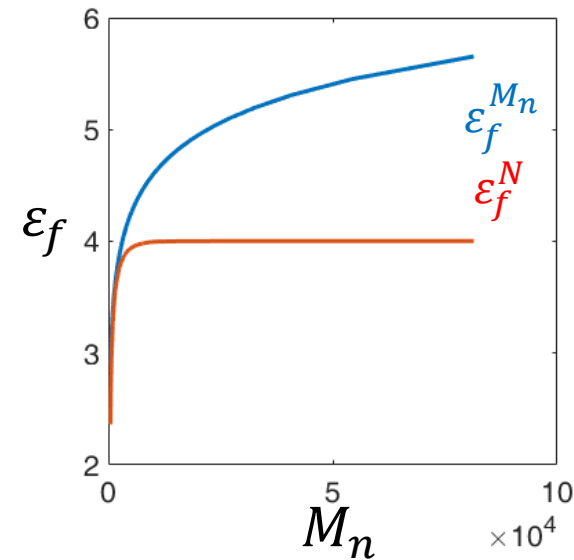


	999	0	0	...
	1020	0	0	...
	398	640	2	...
	1060	0	0	...
	1079	0	0	...
	⋮	⋮	⋮	...

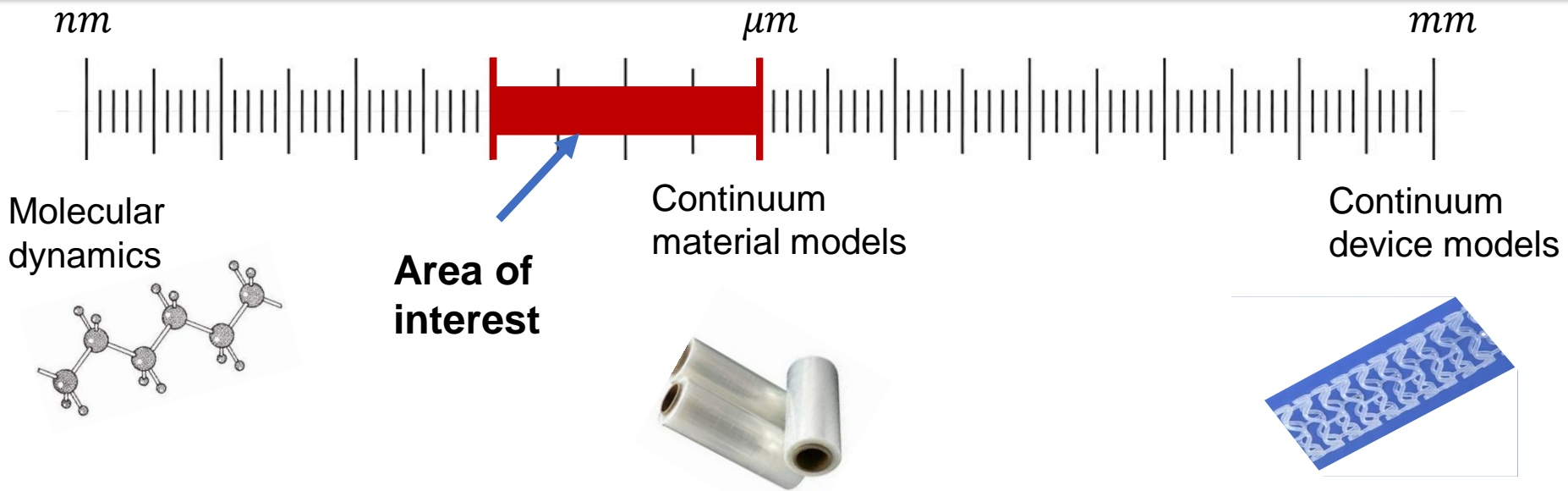
Wang et al., 2008:

$$\frac{\partial M_n}{\partial t} = - (k_1 M_n + k_2 M_n C_m^\beta)$$

$$\frac{\partial C_m}{\partial t} = k_1 M_n + k_2 M_n C_m^\beta + \nabla \cdot (D \nabla C_m)$$



Further work

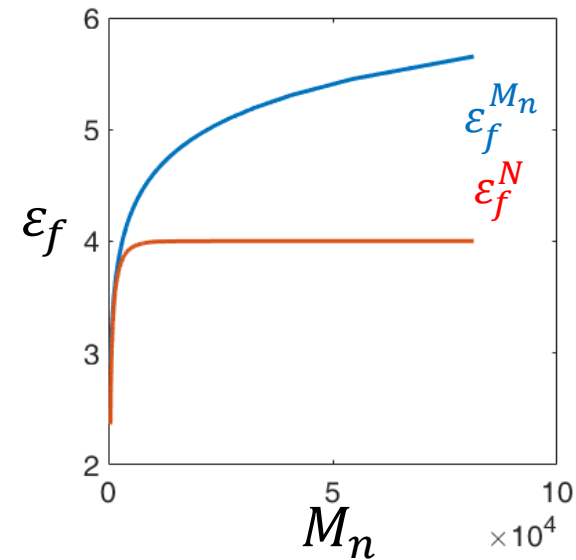


(999	0	0	...
	1020	0	0	...
	398	640	2	...
	1060	0	0	...
	1079	0	0	...
	⋮	⋮	⋮	...

Wang et al., 2008:

$$\frac{\partial M_n}{\partial t} = - (k_1 M_n + k_2 M_n C_m^\beta)$$

$$\frac{\partial C_m}{\partial t} = k_1 M_n + k_2 M_n C_m^\beta + \nabla \cdot (D \nabla C_m)$$



References

R. N. Shirazi, W. Ronan, Y. Rochev, P. E. McHugh.

Modelling the degradation and elastic properties of poly(lactic-co-glycolic acid) films and regular open-cell tissue engineering scaffolds.

Journal of the Mechanical Behavior of Biomedical Materials, **54**:48-59, 2016.

K. S. Bezela.

Examination of biodegradable materials for medical devices.

Unpublished ME thesis. RWTH Aachen University; National University of Ireland, Galway, 2017.

Q. Luo, X. Liu, Z. Li, C. Huang, W. Zhang, J. Meng, Z. Chang, Z. Hua.

Degradation Model of Bioabsorbable Cardiovascular Stents.

PLoS ONE, **9**(11):e110278, 2014.

B. Fayolle, L. Audouin, J. Verdu.

A critical molar mass separating the ductile and brittle regimes as revealed by thermal oxidation in polypropylene.

Polymer, **45**:4324-4330, 2004.

Y. Wang, J. Pan, X. Han, et al.

A phenomenological model for the degradation of biodegradable polymers.

Biomaterials, **29**(23):3393-3401, 2008.